

---

01 **Computational Neuroscience**

02  
03  
04  
05  
06  
07  
08 **By**

09  
10 **WANPRACHA CHAOVALITWONGSE**  
11 Rutgers University, Piscataway, NJ, USA

12  
13 **PANOS M. PARDALOS**  
14 University of Florida, Gainesville, FL, USA

15  
16  
17 **PETROS XANTHOPOULOS**  
18 University of Florida, Gainesville, FL, USA

01 *Editors*

02 Wanpracha Chaovalitwongse  
03 Department of Industrial and  
04 Systems Engineering  
05 Rutgers State University of  
06 New Jersey  
07 96 Frelinghuysen Rd.  
08 Piscataway NJ 08854  
09 USA  
10 wchaoval@rci.rutgers.edu

11 Petros Xanthopoulos  
12 Department of Industrial and  
13 Systems Engineering  
14 University of Florida  
15 303 Weil Hall P.O.Box 116595  
16 Gainesville FL 32611-6595  
17 USA  
18 petrosx@ufl.edu

Panos M. Pardalos  
Department of Industrial and  
Systems Engineering  
University of Florida  
303 Weil Hall  
Gainesville FL 32611-6595  
USA  
pardalos@ise.ufl.edu

21  
22  
23  
24  
25  
26  
27  
28 ISSN 1931-6828  
29 ISBN 978-0-387-88629-9 e-ISBN 978-0-387-88630-5  
30 DOI 10.1007/978-0-387-88630-5  
31 Springer New York Dordrecht Heidelberg London

32 Library of Congress Control Number: 2010920236

33  
34 Mathematics Subject Classification (2000): 92-08, 92C55

35  
36 © Springer Science+Business Media, LLC 2010

37 All rights reserved. This work may not be translated or copied in whole or in part without the written  
38 permission of the publisher (Springer Science+Business Media, LLC, 233 Spring Street, New York,  
39 NY 10013, USA), except for brief excerpts in connection with reviews or scholarly analysis. Use in  
40 connection with any form of information storage and retrieval, electronic adaptation, computer software,  
41 or by similar or dissimilar methodology now known or hereafter developed is forbidden.

42 The use in this publication of trade names, trademarks, service marks, and similar terms, even if they are  
43 not identified as such, is not to be taken as an expression of opinion as to whether or not they are subject to  
44 proprietary rights.

45 Printed on acid-free paper

Springer is part of Springer Science+Business Media (www.springer.com)

01 **Chapter 2**

02 **Investigating Functional Cooperation in the**  
03 **Human Brain Using Simple Graph-Theoretic**  
04 **Methods**  
05  
06  
07

08 Michael L. Anderson, Joan Brumbaugh, and Aysu Şuben  
09  
10  
11  
12  
13  
14

15 **Abstract** This chapter introduces a very simple analytic method for mining large  
16 numbers of brain imaging experiments to discover functional cooperation between  
17 regions. We then report some preliminary results of its application, illustrate some  
18 of the many future projects in which we expect the technique will be of considerable  
19 use (including a way to relate fMRI to EEG), and describe a research resource for in-  
20 vestigating functional cooperation in the cortex that will be made publicly available  
21 through the lab web site. One significant finding is that differences between cogni-  
22 tive domains appear to be attributable more to differences in patterns of cooperation  
23 between brain regions, rather than to differences in which brain regions are used in  
24 each domain. This is not a result that is predicted by prevailing localization-based  
25 and modular accounts of the organization of the cortex.  
26  
27  
28

29 **2.1 Introduction and Background**  
30

31 Hardly an issue of science or nature goes by without creating a stir over the dis-  
32 covery of “the” gene for some disease, trait, or predisposition, or “the” brain area  
33 responsible for some behavior or cognitive capacity. Of course, we know better; the  
34 isolable parts of complex systems like the brain or the human genome do what they  
35 do only in virtue of the cooperation of very many other parts, and often only by  
36 operating within and taking advantage of specific environmental and developmental  
37

---

38 Michael L. Anderson

39 Department of Psychology, Franklin and Marshall College, Lancaster, PA 17604, USA; Institute  
40 for Advanced Computer Studies, University of Maryland, College Park, MD 20742, USA,  
41 e-mail: michael . anderson@fandm . edu

42 Joan Brumbaugh

43 Department of Psychology, Franklin and Marshall College, Lancaster, PA 17604, USA

44 Aysu Şuben

45 Department of Psychology, Franklin and Marshall College, Lancaster, PA 17604, USA

01 contexts. But while it is true that we have gotten better about acknowledging the  
02 limitations of our instinctive reductionism – a bit of humility that the media would  
03 do well to absorb into its reporting – actual scientific practice has yet to be much  
04 affected by awareness of those limits. A recent case in point is John Anderson’s  
05 project to map ACT-R components to brain regions [3]. The motivations for the  
06 project are of course entirely sound: if ACT-R is to be a realistic model of human  
07 cognition, then that model ought to have some significant, testable relationship to  
08 the neural bases of cognition. In this particular set of experiments, the authors identify  
09 eight ACT-R modules and match each one to a different region of interest. They  
10 then look for, and find, significant fit between the predictions for the BOLD signal in  
11 those regions, based on the activity of the ACT-R modules while solving a particular  
12 arithmetic task, and the measured BOLD signal in human participants performing  
13 the same task. On its face, this is an intriguing result and seems to offer compelling  
14 support for the ACT-R model. But the methodological assumption of the project –  
15 that there is a 1:1 mapping of ACT-R modules and brain areas – is highly suspect.  
16 Nor are the authors unaware of this difficulty, and in fact they specifically caution  
17 against making any inference from their approach to the functional organization of  
18 the brain:

20 Some qualifications need to be made to make it clear that we are not proposing  
21 a one-to-one mapping between these eight regions and the eight functions.  
22 First, other regions also serve these functions. Many areas are involved in vision  
23 and the fusiform gyrus has just proven to be the most useful to monitor.  
24 Similarly, many regions have been shown to be involved in retrieval, particularly  
25 the hippocampus. The prefrontal region is just the easiest to identify and seems  
26 to afford the best signal-to-noise ratio. Equally, we are not claiming these regions  
27 only serve one function. This paper has found some evidence for multiple functions.  
28 For instance, the motor regions are involved in rehearsal as well as external action  
29 (213–4).

32 Although we should appreciate the authors’ candor here, the caveat seriously  
33 undermines the ability to interpret their results. If from the discovery that activity  
34 in an ACT-R module predicts the BOLD signal in specific brain region, we can  
35 neither infer that the region serves that specific function (because it is also activated  
36 in other tasks), nor that the function is served by that region (because other regions  
37 are activated by the target task), then we are not left with much. And yet despite  
38 the authors’ awareness of these problems, they stick by the methodology that causes  
39 them.

40 Why might this be so? Naturally, all scientists are faced with the necessity of  
41 making simplifying abstractions to increase the tractability of their work; but as the  
42 authors found themselves, the assumption of a 1:1 mapping of modules to brain  
43 areas is not an approximation to reality, but appears to be fundamentally misleading.  
44 So what would account for the fact that they persist in applying methodological  
45 assumptions that they know to be inadequate? Given the scientific stature of the

01 authors, the question prompts reflection on the range and adequacy of the method-  
02 ological tools actually available for work in this area. One sticks with improper tools  
03 only when the other options appear even worse. And while there are indeed more  
04 sophisticated tools for cooperation-sensitive investigations of neuroscientific data,  
05 those techniques are typically highly complex, hard to master, and – most impor-  
06 tantly – produce results that can be difficult to interpret.

07 To help address these related problems, this chapter will describe a very simple  
08 analytical technique that we have been using in our lab to make cooperation-  
09 sensitive investigations tractable. In this chapter, we will outline that method, report  
10 some preliminary results of its application, and illustrate some of the many future  
11 projects in which we expect this technique (and the underlying database of brain  
12 imaging studies) will be of considerable use.

## 15 2.2 Graph Theory and Neuroscience

17 A graph is a set of objects called points, vertices, or nodes connected by links  
18 called lines or edges. Graphs have proven to be a convenient format to represent  
19 relationships in very many different areas, including computer networks, telephone  
20 calls, airline route maps, and social interactions [18, 19]. In neuroscience, graphs  
21 have been used for such purposes as investigating neural connectivity patterns [27],  
22 correcting brain images [17], and analyzing the patterns of neural activations in  
23 epilepsy [32]. Nevertheless graphs and graph theory – the branch of mathematics  
24 concerned with exploring the topological properties of graphs [15] – remain at this  
25 time underutilized tools with enormous potential to advance our understanding of  
26 the operations of the brain.

28 Our approach to investigating functional cooperation in the cortex involves build-  
29 ing co-activation graphs, based on applying some simple data analysis techniques  
30 to large numbers of brain imaging studies. The method consists of two steps: first,  
31 choosing a spatial segmentation of the cortex to represent as nodes (current work  
32 uses Brodmann areas, but alternate segmentation schemes could easily be used; see  
33 below); and second, performing some simple analyses to discover which regions –  
34 which nodes – are statistically likely to be co-active. These relationships are repre-  
35 sented as edges in our graphs.

36 For this second step we proceed in the following way. Given a database of brain  
37 imaging studies containing information about brain activations in various contexts  
38 (we describe the particular database we have been using in the next section), we  
39 first determine the chance likelihood of activation for each region by dividing the  
40 number of experiments in which it is reported to be active by the total number of  
41 experiments in the database. Then, for each pair of regions, we use a  $\chi^2$  measure  
42 to determine if the regions are more (or less) likely to be co-active than would be  
43 predicted by chance. We also perform a binomial analysis, since a binomial measure  
44 can provide directional information. (It is sometimes the case that, while area A and  
45 area B are co-active more (or less) often than would be predicted by chance, the

effect is asymmetric, such that area B is more active when area A is active, but not the reverse.)

Figure 2.1 shows the results of one such analysis, for a set of action and attention tasks. The graphs represent Brodmann areas that are significantly more likely than chance to be co-active ( $\chi^2 > 3.84$ ); it is hypothesized that the network of co-activated areas revealed by such analysis represents those areas of the cortex that cooperate to perform the cognitive tasks in the given domain. The co-activation graphs are superimposed on an adjacency graph (where edges indicate that the Brodmann areas share a physical border in the brain) for ease of visual comparison.

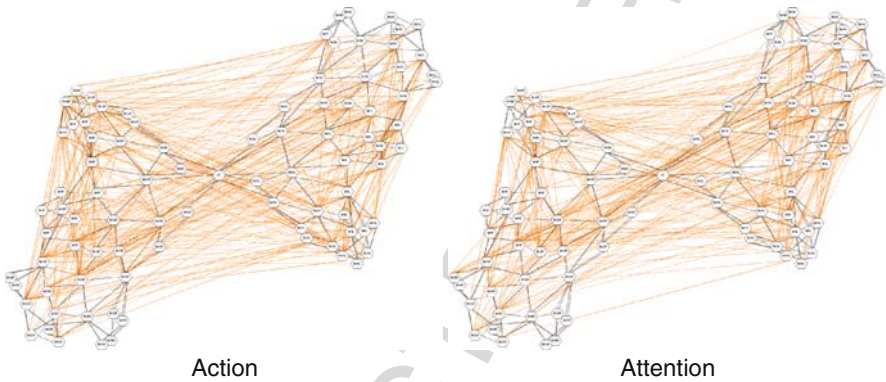


Fig. 2.1: Cortex represented as adjacency + co-activation graphs. Here the Brodmann areas are nodes, with *black lines* between adjacent areas and *orange lines* between areas showing significant co-activation. The graph on the *top* shows co-activations from 56 action tasks, and the graph on the *bottom* shows co-activations from 77 attention tasks. Edges determined using the threshold  $\chi^2 > 3.84$ . Graphs rendered with aiSee v. 2.2.

Note that co-activation analysis is similar to, but distinct from, the approach adopted by [31] in discovering “functional connectivity.” The main difference is that edges in functional connectivity graphs indicate temporal co-variation between brain regions. Moreover, the results they report generally represent the dynamics of simulated neural networks (based on the structure of biological brain networks), rather than the static analysis of data-mining imaging experiments. Hence we adopt the term “functional cooperation” to distinguish our results from theirs. Nevertheless, there is presumably much to be gained by leveraging both sorts of analysis; in a later section we describe one such future project for bringing co-activation and co-variation graphs together.

The results of such analysis are not just visually striking, but afford the application of some well-understood mathematical techniques to better understand features of brain organization and functional cooperation. Of course, exactly what sorts of

01 techniques are appropriate, and how the end results should be interpreted, depend a  
02 great deal on the nature of the underlying data. Thus, in the next section we de-  
03 scribe the database that we have been working with and how other researchers  
04 can get access to it for their own use. Then, in the final section, we will describe  
05 some of the projects to which we have applied this resource and some of the future  
06 possibilities.

### 09 **2.3 A Database of Imaging Experiments**

11 Over the last year or so we have compiled a database containing 665 experiments  
12 in 18 cognitive domains. The database currently consists of every qualifying imag-  
13 ing study in the *Journal of Cognitive Neuroscience* from 1996 to 2006, as well as  
14 the 135 experiments from [11] that were used in previous studies [4, 6]. To qual-  
15 ify for inclusion in the database, the study had to be conducted on healthy adults  
16 and to use a subtraction-based methodology for analyzing results. The database  
17 contains only post-subtraction activations. The data recorded for each experiment  
18 include the publication citation, the domain and sub-domain, the imaging method,  
19 the Talairach coordinates of each reported activation, the Brodmann area of each  
20 reported activation, the relative placement of the activation in the Brodmann area  
21 (e.g., frontal, caudal, ventral, dorsal), and the comparison used to generate the re-  
22 sults. The domain labels are consistent with those used by the BrainMap database  
23 [22]. For experiments where coordinates were reported in MNI coordinates, a soft-  
24 ware package called GingerALE was used to translate these into Talairach co-  
25 ordinates [21]. When the authors of the study reported the Brodmann areas of  
26 their activations, these were recorded as reported. Where the authors did not re-  
27 port Brodmann areas, a software package called the Talairach demon [24] was  
28 used to provide Brodmann area labels for the coordinates. This program reports  
29 a distance in millimeters from the coordinate to the reported Brodmann area; this  
30 is the range, and it is recorded in cases where the BA label was generated us-  
31 ing the software. The range is useful for excluding from analysis Brodmann area  
32 labels for coordinates that are further than desired from the reported area. Our  
33 plans are to continue to add to the database and analysis, and to publish ver-  
34 sions at 1 year intervals beginning in the fall of 2008. The published versions of  
35 the database will contain the base data detailed above, as well as co-activation  
36 graphs, and will be prepared according to the following procedure: first, we will  
37 only include in the co-activation analysis sample domains containing some mini-  
38 mum number of experiments (e.g., 50 or 100, to be determined by what is feasi-  
39 ble given the state of the database at that time). Having identified these domains,  
40 we will generate a concordance of authors to be sure that no individual labs are  
41 overrepresented in any given domain. The samples will be balanced by lab by  
42 randomly excluding experiments from overrepresented authors. At this point we  
43 will choose a target  $n$  based on the number of experiments in the domain contain-  
44 ing the fewest number of experiments. An equal number of experiments will be  
45

01 randomly selected from the remaining domains. This set of experiments, equally  
02 balanced between the domains, will be the sample for that year’s co-activation  
03 analysis.

04 On this balanced sample we will run at least the following kinds of analysis.  
05 (1) For each domain, and for the entire set, we will generate a co-activation graph,  
06 constructed using the method outlined above, using Brodmann areas as nodes, and  
07 including only activations with a range (see above) of less than 5 mm. The calculated  
08 chance of activation and co-activation, as well as the binomial probability and  $\chi^2$   
09 value will be reported for each pair of Brodmann areas, allowing researchers to  
10 set their own probability thresholds. (2) For each of the co-activation graphs, we  
11 will do a clique analysis (see below). Lancaster et al. [23] reviews some methods  
12 for generating cliques from brain activation data, and there are many other well-  
13 established methods for extracting cliques of various descriptions from graphs [1,  
14 8, 9, 16]. Finally, (3) for all of the co-activation graphs and cliques, we will project  
15 them onto the adjacency graph (shown above) and calculate the average minimum  
16 graph distance (the “scatter” in the cortex) of the included nodes. All of this data  
17 will be made available for download from the lab web site, at

18 [http://www.agcognition.org/brain\\_network](http://www.agcognition.org/brain_network)

19 Before moving on to the next section, where we describe some of the uses to  
20 which these data have been put, and how it can be applied in the future, it is worth  
21 saying a word about our reliance on Brodmann areas as the basis for the analy-  
22 ses. It is of course legitimate to wonder whether the sub-division of the cortex  
23 into Brodmann areas will be a feature of our final functional map of the human  
24 brain; one rather suspects it will be fully superseded by some yet-to-be developed  
25 topographical scheme. Yet Brodmann areas remain the lingua franca in Cognitive  
26 Neuroscience for reporting findings, and sticking to this tradition will make results  
27 using these analyses easier to relate to past findings. Moreover, for the purposes  
28 we have described here – investigating the functional cooperation between brain  
29 areas involved in supporting different functions – virtually any consistent spatial  
30 division of the brain will do, and regions the size of Brodmann areas offer ade-  
31 quate spatial resolution for the required analysis. For, while the spatial resolution  
32 of a single fMRI image is on the order of 3 mm or better, there are questions both  
33 about the accuracy and precision of repeated fMRI, both within and between par-  
34 ticipants, effectively reducing its functional resolution [28]. It is arguable, then, that  
35 the use of Brodmann-sized regions of the cortex for representing the contribution  
36 of individual brain areas to cognitive tasks is consistent with the realistic (con-  
37 servatively estimated) spatial resolution of current imaging technologies [10, 34].  
38 In any case, it should be noted that the coordinates of each activation are also  
39 recorded in the database; if a Brodmann-based spatial scheme does not appear to  
40 produce useful or legitimate results, other spatial divisions of the cortex can cer-  
41 tainly be substituted, and the very same sort of analysis performed. For instance,  
42 one can use the ALE (activation likelihood estimates) paradigm [33] to extract prob-  
43 able activations for arbitrarily defined neural volumes and build graphs from these  
44 data [23].



## 2.4 The Usefulness of Co-activation Graphs

With brain imaging data in this format, it becomes possible to formulate some very simple questions and use some well-understood methods to answer them. For instance, a long-standing project in our lab has been adjudicating between functional topographies of the brain based on the principle of localization and those based on the principle of redeployment. Localization-based approaches to functional topography, insofar as they typically expect brain regions to be dedicated to a small and domain-restricted set of cognitive functions, would be committed to the notion that differences in cognitive domains would be reflected primarily in differences in which brain regions support tasks in the domain. In contrast, redeployment-based approaches, being based on the idea that most brain regions are used in many different tasks across cognitive domains, would expect very little difference in which brain regions were used in each domain. However, because redeployment nevertheless expects brain regions to have fixed low-level functions [3–5], it is committed to the notion that differences in functions and domains must instead be the result of differences in the ways in which the areas cooperate in supporting different tasks. To put this in more concrete visual terms, imagine a simplified brain with six regions that together support two different cognitive domains. If one supports a localization-based (or a classical modular) organization for the brain, one would expect the regional cooperation patterns to look like those in the diagram on the left. In contrast, redeployment predicts an organization that looks something more like that shown in the diagram on the right (Fig. 2.2).

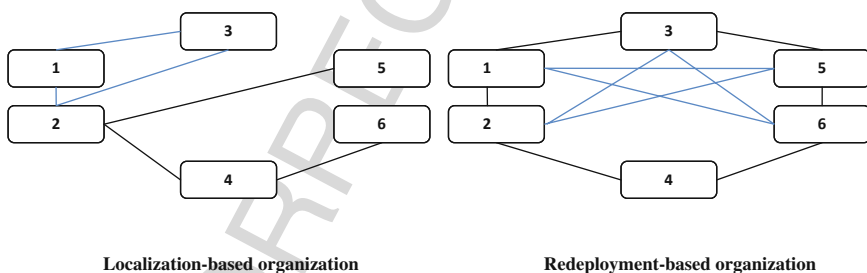
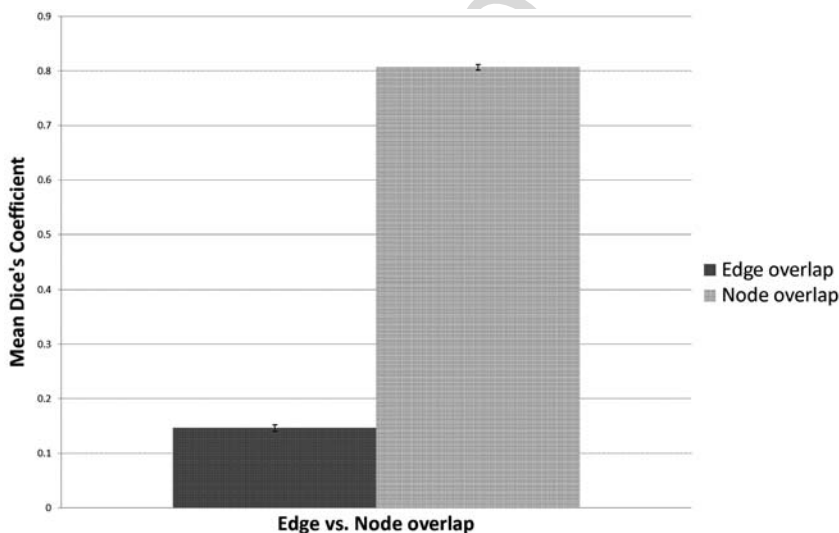


Fig. 2.2: Two different possibilities for the functional organization of the cortex. Figure shows an imagined brain with six regions supporting two cognitive domains. Localization predicts that domain 1 (*blue*) and domain 2 (*black*) will utilize different brain areas, while redeployment predicts that the domains will utilize many of the same brain areas, cooperating in different patterns.

There is an obvious analog for these features in our co-activation graphs: comparing the graphs from different domains, node overlaps indicate Brodmann areas that support tasks in both domains, whereas edge overlaps would indicate a similar pattern of cooperation between Brodmann areas. Thus, localization predicts little node

01 overlap between co-activation graphs (and therefore also low edge overlap), while  
 02 redeployment predicts a great deal of node overlap, but little edge overlap. Using  
 03 our database of imaging data, we did a co-activation analysis for the eight cognitive  
 04 domains having more than 30 experiments: action; attention; emotion; language;  
 05 memory; mental imagery; reasoning; and visual perception. The number of experi-  
 06 ments (472 total) was not balanced between domains and authors, but otherwise  
 07 followed the procedures outlined above. Using Dice's coefficient as our measure  
 08 ( $d = 2(o_{1,2}) / (n_1 + n_2)$ , where  $o$  is the number of overlapping elements and  $n$  is  
 09 the total number of elements in each set), we compared the amount of node and  
 10 edge overlap between each of the eight domains. As predicted by redeployment, we  
 11 found a high degree of node overlap ( $d = 0.81$ ,  $SD = 0.04$ ) but very little edge over-  
 12 lap ( $d = 0.15$ ,  $SD = 0.04$ ). The difference is significant (two-sample Student's- $t$  test,  
 13 double-sided  $p \ll 0.001$ ). Figure 2.3 shows a graph of the results. This is just one  
 14 among a number of findings that suggest that redeployment is the better supported  
 15 approach to understanding the functional topography of the cortex [4–6].



34  
 35 Fig. 2.3: Mean overlap of nodes vs. edges. A graph of the average Dice's coefficient  
 36 for similarity between the sets of nodes and edges in a pair-wise comparison of co-  
 37 activation graphs from eight cognitive domains. Difference between the means is  
 38 significant ( $p \ll 0.001$ ).

39  
 40 Looking at node and edge overlaps is just a simple example of the sorts of compar-  
 41 isons one might make using data in this format. Others more specific to graph-  
 42 based representations also readily suggest themselves. For instance, one common  
 43 form of analysis in graphs is a clique analysis, so called because of its origin in the  
 44 analysis of social networks [2]. A clique is a maximal complete sub-graph – that  
 45

01 is, a set of nodes in a graph that are fully connected with one another, but not fully  
02 connected with any other node in the whole graph. In this context, a clique would  
03 indicate a set of Brodmann areas that are fully co-active with each other, but not  
04 with other areas of the brain; any such neural cliques would obviously be structures  
05 of interest. As in the case of social networks, however, this definition may be too  
06 strict for many purposes. Intuitively, we would be interested in sets of nodes that are  
07 cohesive and relatively isolated – that is, nodes that are highly but not necessarily  
08 fully connected, and much more connected with each other than with other nodes in  
09 the graph. These would represent sets of brain regions that are generally co-active  
10 with each other, but that operate with relative independence from the rest of the  
11 brain. Alba [2] offers the notion of a sociometric clique (an  $n$ -clique of diameter  $n$ ),  
12 as well as measures of cohesiveness and isolation, that could be adopted here to  
13 discover sets of brain regions with the desired properties. Cohesive, isolated socio-  
14 metric cliques seem likely to correspond to the neural components that cooperate to  
15 support a set of closely related cognitive functions or sub-functions. Whether this is  
16 so is an open scientific question, but such cliques are a far more plausible target for  
17 investigations into the neural components supporting particular cognitive functions  
18 than are individual brain areas. To return us to the issue with which this chapter be-  
19 gan: co-activation graphs allow one to discover (among other things) neural cliques;  
20 in our view, what Anderson et al. should be doing is trying to match ACT-R modules  
21 to these sorts of structures, and not to individual brain areas.

22 These are far from the only research avenues that these data offer. One can also  
23 look at other features of the graphs, such as local topography, which may help make  
24 plausible inferences about underlying function. For instance, a hub-and-spoke pat-  
25 tern of co-activation may indicate broadcast or information consolidation functions;  
26 in contrast, long strings of connected nodes might indicate serial processing.

27 We could go on indefinitely, but the point is not to exhaustively list all the possi-  
28 ble analyses one might make with graph-based co-activation data. Instead we would  
29 like to take the opportunity to call to mind the fact that, at very many points in  
30 the history of science, great progress has been made just in virtue of finding the  
31 right format for otherwise well-known data. In a field as young as Cognitive Neu-  
32 roscience it is still more than possible for simple ideas to make a transformative  
33 impact; co-activation graphs may be one of those ideas.

## 36 2.5 Relating fMRI to EEG

38 We would like to conclude by describing one longer term application of co-  
39 activation graphs about which we are especially excited. As the reader is no doubt  
40 aware, a long-standing issue in experimental and clinical neuroscience has been the  
41 question of how to relate data from EEG/MEG to fMRI. Chief among the many ob-  
42 stacles standing in the way of relating the two have been (1) questions over whether  
43 each technology measures the same underlying neural activity [26] and (2) difficulty  
44 in finding the right representational format for the relation, given the vastly differ-  
45

01 ent temporal scale of the two data streams [20]. However, recent research seems to  
02 indicate a mitigation of the first issue; and co-activation graphs may contribute to a  
03 novel approach to the second. We will discuss each of these in turn.

04 Although there have been for some time, and continue to be, questions about the  
05 neurophysiological bases of the fMRI signal, converging evidence strongly suggests  
06 that the BOLD signal is best correlated with local field potentials [25, 7, 35]. This  
07 is good news for the project of relating EEG and fMRI, because recent work has  
08 shown that EEG signals can also be analyzed to give estimations of LFP [29, 30].  
09 Although this is hardly to be considered the last word on the subject, it appears  
10 that differences in underlying neurophysiological basis do not necessarily pose an  
11 obstacle to relating the two sources of data.

12 This brings us to the vast differences in temporal resolution. Since existing fMRI  
13 data cannot be made faster, typical solutions to the mismatch in temporal resolu-  
14 tion have involved lowering the resolution of the EEG signal, by sampling signals  
15 over much longer timescales, and applying mathematical or statistical procedures  
16 (e.g., temporal averaging) to generate a relevant structure such as a local maximum  
17 in the 3D current distribution; this can then be compared to equivalent structures  
18 from fMRI. Vitacco et al. [36] applied this method to relate EEG and fMRI in a  
19 word classification task, but while they were able to obtain agreement between local  
20 maxima for group mean data, there was much poorer correspondence for individ-  
21 ual subjects. One reason for this problem may be that, in averaging or otherwise  
22 manipulating EEG signals, one may be generating artifacts rather than discovering  
23 real features of the data. This is not to say that such attempts at data fusion are not  
24 promising, only that there is room for the introduction and evaluation of alternate  
25 approaches.

26 We have already outlined our approach to mining large numbers of fMRI studies  
27 and representing the results in graph format. This is relevant to the current issue be-  
28 cause Chaovalitwongse et al. [13] recently developed a way to represent EEG data  
29 that also emphasized cooperative activity and also involved a graph-based repre-  
30 sentation scheme. In the scheme developed by Chaovalitwongse et al., cooperation  
31 between brain areas is measured in terms of the co-variance between EEG elec-  
32 trodes. Although the discovery of temporal correlation in large data sets is far from  
33 a trivial problem. Chaovalitwongse et al. [14, 12] have developed different methods  
34 to make such data mining tractable.

35 In discussions with Prof. Chaovalitwongse, we quickly realized that combining  
36 our two approaches could help address the issue of relating fMRI and EEG, because  
37 in approaches that focus on the cooperation of brain areas the small-scale temporal  
38 features of the EEG signal are de-emphasized, and the graph-based representational  
39 formats are entirely compatible; given the same underlying spatial segmentation of  
40 the cortex, the two cooperation graphs can be directly overlaid.

41 Of course, while it is clear that co-activation and co-variation graphs can be easily  
42 overlaid, what is unknown is whether there is any systematic relation between EEG  
43 co-variance and fMRI co-activation. We are currently putting together a research  
44 project to help answer this question (insofar as each graph is providing genuine  
45 information about which brain areas cooperate in supporting various cognitive tasks,

01 it certainly seems plausible that there would be some such relation). While it is  
02 by no means certain that any such relation will be found, the potential payoff is  
03 enormous. Among other things, it suggests it would be possible to mine the vast  
04 trove of fMRI data to provide baseline expectations for normal brain function in  
05 terms of the temporal correlation between brain areas. Since this can be observed  
06 cheaply, noninvasively, and in real time with EEG, it would be of great use in clinical  
07 settings for detecting deviations from normal function, such as might be observed  
08 prior to the onset of an epileptic seizure [12].  
09  
10

## 11 2.6 Conclusion

12 This chapter introduced a very simple analytical method for mining large numbers  
13 of brain imaging experiments to discover functional cooperation between brain re-  
14 gions. We reported some preliminary results of its application, illustrated some of  
15 the many future projects in which we expect the technique will be of considerable  
16 use, and described a research resource for investigating functional cooperation in the  
17 cortex that will be made publicly available through the lab web site. We hope and  
18 expect the availability of this resource will help spur new and innovative discoveries  
19 in the cognitive and computational neurosciences.  
20  
21  
22  
23

## 24 References

- 25 1. Abello, J., Pardalos, P.M., Resende, M.G.C. On maximum clique problems in very large  
26 graphs in external memory algorithms. In: Abello, J., Vitter, J. (eds.) AMS-DIMACS Series  
27 on Discrete Mathematics and Theoretical Computer Science, Vol. 50 (1999)
- 28 2. Alba, R.D. A graph-theoretic definition of a sociometric clique. *J Math Sociol* **3**, 113–126  
29 (1973)
- 30 3. Anderson, J.R., Qin, Y., Jung, K.J., Carter, C.S. Information processing modules and their  
31 relative domain specificity. *Cogn Psychol* **54**, 185–217 (2007)
- 32 4. Anderson, M.L. Evolution of cognitive function via redeployment of brain areas. *Neuroscien-*  
33 *tist* **13**(1), 13–21 (2007)
- 34 5. Anderson, M.L. Massive redeployment, exaptation, and the functional integration of cognitive  
35 operations. *Synthese* **159**(3), 329–345 (2007)
- 36 6. Anderson, M.L. The massive redeployment hypothesis and the functional topography of the  
37 brain. *Philos Psychol* **21**(2), 143–174 (2007)
- 38 7. Attwell, D., Iadecola, C. The neural basis of functional brain imaging signals. *Trends Neurosci*  
39 **25**(12), 621–25 (2002)
- 40 8. Bock, R.D., Husain, S.Z. An adaptation of Holzinger's b-coefficients for the analysis of so-  
41 ciometric data. *Sociometry* **13**, 146–53 (1950)
- 42 9. Bonacich, P. Factoring and weighting approaches to status scores and clique identification. *J*  
43 *Math Sociol* **2**, 113–20 (1972)
- 44 10. Brannen, J.H., Badie, B., Moritz, C.H., Quigley, M., Meyerand, M.E., Haughton, V.M. Relia-  
45 bility of functional MR imaging with word-generation tasks for mapping Broca's area. *Am J*  
*Neuroradiol* **22**, 1711–1718 (2001)
11. Cabeza, R., Nyberg, L. Imaging cognition II: An empirical review of 275 PET and fMRI  
studies. *J Cogn Neurosci* **12**, 1–47 (2000)

12. Chaovalitwongse, W., Fan, Y.J., Sachdeo, R. On the k-nearest dynamic time warping neighbor for abnormal brain activity classification. *IEEE Trans Syst Man Cybern A Syst Hum* **37**(6), 1005–1016 (2007). To appear
13. Chaovalitwongse, W., Iasemidis, L.D., Pardalos, P.M., Carney, P.R., Shiau, D.S., Sackellares, J.C. Performance of a seizure warning algorithm based on the dynamics of intracranial EEG. *Epilepsy Res* **64**, 93–133 (2005)
14. Chaovalitwongse, W., Pardalos, P.M., Prokopyev, O.A. Electroencephalogram (EEG) time series classification: Applications in epilepsy. *Ann Operations Res* **148**, 227–250 (2006)
15. Diestel, R. *Graph Theory*, 3rd edn. Springer-Verlag, Heidelberg (2005)
16. Gross, J.L., Yellen, J. *Graph Theory and its Applications*, 2nd edn. Discrete Mathematics and Its Applications. Chapman & Hall/CRC, London (2005)
17. Han X., Xu, C., Braga-Neto, U., Prince, J.L. Topology correction in brain cortex segmentation using a multiscale, graph-based approach. *IEEE Trans Med Imaging* **21**, 109–121 (2002)
18. Hayes, B. Graph theory in practice: Part I. *Am Sci* **88**(1), 9–13 (2000)
19. Hayes, B. Graph theory in practice: Part II. *Am Sci* **88**(2), 104–109 (2000)
20. Horwitz, B., Poeppel, D. How can EEG/MEG and fMRI/PET data be combined? *Hum. Brain Mapp.* **17**, 1–3 (2002)
21. Laird, A.R., Fox, M., Prince, C.J., Glahn, D.C., Uecker, A.M., Lancaster, J.L., Turkeltaub, P.E., Kochunov, P., Fox, P.T. Ale meta-analysis: Controlling the false discovery rate and performing statistical contrasts. *Hum Brain Mapp* **25**, 155–164 (2005)
22. Laird, A.R., Lancaster, J.L., Fox, P.T. Brainmap: The social evolution of a functional neuroimaging database. *Neuroinformatics* **3**, 65–78 (2005)
23. Lancaster, J., Laird, A., Fox, M., Glahn, D., Fox, P. Automated analysis of meta-analysis networks. *Hum Brain Mapp* **25**, 174–184 (2005)
24. Lancaster, J.L., Woldorff, M.G., Parsons, L.M., Liotti, M., Freitas, C.S., Rainey, L., Kochunov, P.V., Nickerson, D., Mikiten, S.A., Fox, P.T. Automated talairach atlas labels for functional brain mapping. *Hum Brain Mapp* **10**, 120–131 (2000)
25. Logothetis, N.K., Pauls, J., Augath, M., Trinath, T., Oeltermann, A. Neurophysiological investigation of the basis of the fMRI signal. *Nature* **412**, 150–157 (2001)
26. Nunez, P.L., Silberstein, R.B. On the relationship of synaptic activity to macroscopic measurements: Does co-registration of EEG with fMRI make sense? *Brain Topogr* **13**, 79–96 (2000)
27. Sporns, O., Ktter, R. Motifs in brain networks. *PLoS Biol* **2**, e369 (2004)
28. Özcan, M., Baumgärtner, U., Vucurevic G. Stoeter, P., Treede, R.D. Spatial resolution of fMRI in the human parasyllvian cortex: Comparison of somatosensory and auditory activation. *NeuroImage* **25**(3), 877–887 (2005)
29. Grave de Peralta Menendez, R., Gonzales Andino, S., Morand, S., Michel, C., Landis, T. Imaging the electrical activity of the brain. *Electra Hum Brain Mapp* **9**, 1–12 (2000)
30. Grave de Peralta Menendez, R., Murray, M.M., Michel, C., Martuzzi, R., Gonzales Andino, S.L. Electrical neuroimaging based on biophysical constraints. *NeuroImage* **21**, 527–539 (2004)
31. Sporns, O., Tononi, G., Edelman, G.M. Theoretical neuroanatomy: Relating anatomical and functional connectivity in graphs and cortical connection matrices. *Cereb Cortex* **10**, 127–141 (2000)
32. Suharitdamrong, W., Chaovalitwongse, A., Pardalos, P.M. Graph theory-based data mining techniques to study similarity of epileptic brain network. In: *Proceedings of DIMACS Workshop on Data Mining, Systems Analysis, and Optimization in Neuroscience* (2006)
33. Turkeltaub, P.E., Eden, G.F., Jones, K.M., Zeffiro, T.A. Meta-analysis of the functional neuroanatomy of single-word reading: Method and validation. *Neuroimage* **16**, 765–780 (2002)
34. Ugurbil, K., Toth, L., Kim, D.S. How accurate is magnetic resonance imaging of brain function? *Trends Neurosci.* **26**(2), 108–114 (2003)
35. Viswanathan, A., Freeman, R.D. Neurometabolic coupling in cerebral cortex reflects synaptic more than spiking activity. *Nat Neurosci* **10**(10), 1308–1312 (2007)
36. Vitacco, D., Brandeis, D., Pausal-Marqui, R., Martin, E. Correspondence of event-related potential tomography and functional magnetic resonance imaging during language processing. *Hum Brain Mapp* **17**, 4–12 (2002)